

Tissue Identification in Ultrasound Images using Rayleigh Local Parameter Estimation

Santiago Aja-Fernández, Marcos Martín-Fernández and Carlos Alberola-López

Laboratorio de Procesado de Imagen



Universidad de Valladolid
Spain

- 1 Introduction
 - Speckle
 - Models for Speckle
 - Aim of the work
- 2 Local Statistics of the Rayleigh distribution
 - The Rayleigh distribution
 - Parameter estimation
- 3 Tissue Identification in Ultrasound Images
 - Initial assumptions
 - Algorithm
- 4 Experiments
 - Synthetic Experiments
 - Experiments with Ultrasound Images
- 5 Conclusions

- 1 Introduction
 - Speckle
 - Models for Speckle
 - Aim of the work
- 2 Local Statistics of the Rayleigh distribution
 - The Rayleigh distribution
 - Parameter estimation
- 3 Tissue Identification in Ultrasound Images
 - Initial assumptions
 - Algorithm
- 4 Experiments
 - Synthetic Experiments
 - Experiments with Ultrasound Images
- 5 Conclusions



Speckle

- Speckle is a kind of granular noise,
- Found in many types of coherent imaging systems: SAR, laser illuminated or ultrasound.

Received signal model

$$Z = Xe^{j\phi} = \sum_{n=1}^N x_i e^{j\phi_i}$$



Speckle

- Speckle is a kind of granular noise,
- Found in many types of coherent imaging systems: SAR, laser illuminated or ultrasound.

Received signal model

$$Z = Xe^{j\phi} = \sum_{n=1}^N x_n e^{j\phi_n}$$



Speckle

- Speckle is a kind of granular noise,
- Found in many types of coherent imaging systems: SAR, laser illuminated or ultrasound.

Received signal model

$$Z = Xe^{j\phi} = \sum_{n=1}^N x_n e^{j\phi_n}$$



Speckle

- Speckle is a kind of granular noise,
- Found in many types of coherent imaging systems: SAR, laser illuminated or ultrasound.

Received signal model

$$Z = Xe^{j\phi} = \sum_{n=1}^N x_i e^{j\phi_i}$$

Statistical models

- 1 Rayleigh: phases are random and independent of the amplitudes, number of scatters large, no periodicity in disposition of the scatters.

$$p(X) = \frac{X}{\sigma^2} e^{-\frac{X^2}{2\sigma^2}} u(X)$$

- 2 Rician distribution (specular component Z_s added).
- 3 K distribution
- 4 Homodyned K distribution.
- 5 Others: Nakagami model, Rician inverse Gaussian and Nakagami inverse Gaussian.

–Logarithmic compression no considered–

Statistical models

- 1 Rayleigh: phases are random and independent of the amplitudes, number of scatters large, no periodicity in disposition of the scatters.

$$p(X) = \frac{X}{\sigma^2} e^{-\frac{X^2}{2\sigma^2}} u(X)$$

- 2 Rician distribution (specular component Z_s added).
- 3 K distribution
- 4 Homodyned K distribution.
- 5 Others: Nakagami model, Rician inverse Gaussian and Nakagami inverse Gaussian.

–Logarithmic compression no considered–

Statistical models

- 1 Rayleigh: phases are random and independent of the amplitudes, number of scatters large, no periodicity in disposition of the scatters.

$$p(X) = \frac{X}{\sigma^2} e^{-\frac{X^2}{2\sigma^2}} u(X)$$

- 2 Rician distribution (specular component Z_s added).
- 3 K distribution
- 4 Homodyned K distribution.
- 5 Others: Nakagami model, Rician inverse Gaussian and Nakagami inverse Gaussian.

–Logarithmic compression no considered–

Statistical models

- 1 Rayleigh: phases are random and independent of the amplitudes, number of scatters large, no periodicity in disposition of the scatters.

$$p(X) = \frac{X}{\sigma^2} e^{-\frac{X^2}{2\sigma^2}} u(X)$$

- 2 Rician distribution (specular component Z_s added).
- 3 K distribution
- 4 Homodyned K distribution.
- 5 Others: Nakagami model, Rician inverse Gaussian and Nakagami inverse Gaussian.

–Logarithmic compression no considered–

Statistical models

- 1 Rayleigh: phases are random and independent of the amplitudes, number of scatters large, no periodicity in disposition of the scatters.

$$p(X) = \frac{X}{\sigma^2} e^{-\frac{X^2}{2\sigma^2}} u(X)$$

- 2 Rician distribution (specular component Z_s added).
- 3 K distribution
- 4 Homodyned K distribution.
- 5 Others: Nakagami model, Rician inverse Gaussian and Nakagami inverse Gaussian.

–Logarithmic compression no considered–

Statistical models

- 1 Rayleigh: phases are random and independent of the amplitudes, number of scatters large, no periodicity in disposition of the scatters.

$$p(X) = \frac{X}{\sigma^2} e^{-\frac{X^2}{2\sigma^2}} u(X)$$

- 2 Rician distribution (specular component Z_s added).
- 3 K distribution
- 4 Homodyned K distribution.
- 5 Others: Nakagami model, Rician inverse Gaussian and Nakagami inverse Gaussian.

–Logarithmic compression no considered–

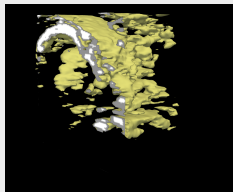
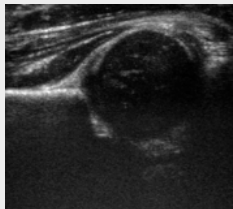
Statistical models

- 1 Rayleigh: phases are random and independent of the amplitudes, number of scatters large, no periodicity in disposition of the scatters.

$$p(X) = \frac{X}{\sigma^2} e^{-\frac{X^2}{2\sigma^2}} u(X)$$

- 2 Rician distribution (specular component Z_s added).
- 3 K distribution
- 4 Homodyned K distribution.
- 5 Others: Nakagami model, Rician inverse Gaussian and Nakagami inverse Gaussian.

–Logarithmic compression no considered–



Assumption

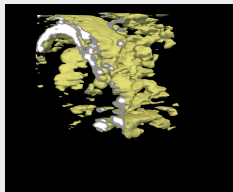
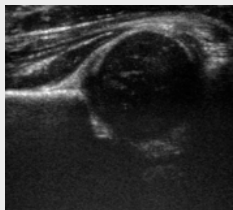
- Rayleigh distribution of the speckle.
- Uniform value of σ for each tissue; different values for different tissues.

Aim

- Estimation of σ in each tissue.
- Classification of pixels according to $\hat{\sigma}$.

Tools

- Local Statistics



Assumption

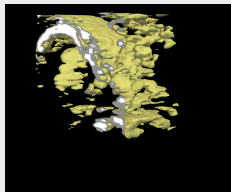
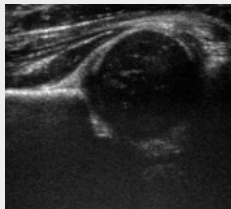
- Rayleigh distribution of the speckle.
- Uniform value of σ for each tissue; different values for different tissues.

Aim

- Estimation of σ in each tissue.
- Classification of pixels according to $\hat{\sigma}$.

Tools

- Local Statistics



Assumption

- Rayleigh distribution of the speckle.
- Uniform value of σ for each tissue; different values for different tissues.

Aim

- Estimation of σ in each tissue.
- Classification of pixels according to $\hat{\sigma}$.

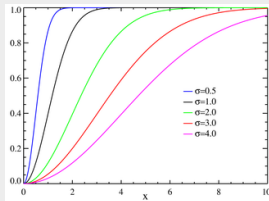
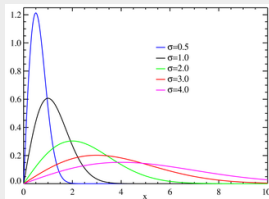
Tools

- Local Statistics

Local Statistics of the Rayleigh distribution

- 1 Introduction
 - Speckle
 - Models for Speckle
 - Aim of the work
- 2 **Local Statistics of the Rayleigh distribution**
 - The Rayleigh distribution
 - Parameter estimation
- 3 Tissue Identification in Ultrasound Images
 - Initial assumptions
 - Algorithm
- 4 Experiments
 - Synthetic Experiments
 - Experiments with Ultrasound Images
- 5 Conclusions

The Rayleigh distribution



PDF

$$p(x|\sigma) = \frac{x}{\sigma^2} e^{-\frac{x^2}{2\sigma^2}} u(x)$$

Moments and parameters

$$\text{Mean: } E\{x\} = \sigma \sqrt{\frac{\pi}{2}}$$

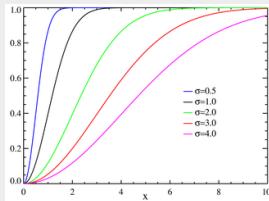
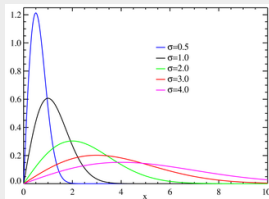
$$\text{Median: } \text{median}\{x\} = \sigma \sqrt{\log(4)}$$

$$\text{Mode: } \text{mode}\{x\} = \sigma$$

$$\text{Variance: } \text{Var}\{x\} = \sigma^2 \frac{4-\pi}{2}$$

$$\text{Second order moment: } E\{x^2\} = 2\sigma^2$$

The Rayleigh distribution



PDF

$$p(x|\sigma) = \frac{x}{\sigma^2} e^{-\frac{x^2}{2\sigma^2}} u(x)$$

Moments and parameters

Mean: $E\{x\} = \sigma \sqrt{\frac{\pi}{2}}$

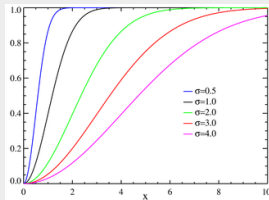
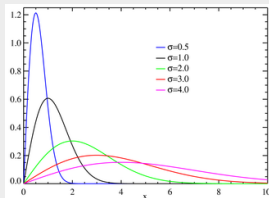
Median: $\text{median}\{x\} = \sigma \sqrt{\log(4)}$

Mode: $\text{mode}\{x\} = \sigma$

Variance: $\text{Var}\{x\} = \sigma^2 \frac{4-\pi}{2}$

Second order moment: $E\{x^2\} = 2\sigma^2$

The Rayleigh distribution



PDF

$$p(x|\sigma) = \frac{x}{\sigma^2} e^{-\frac{x^2}{2\sigma^2}} u(x)$$

Moments and parameters

Mean: $E\{x\} = \sigma \sqrt{\frac{\pi}{2}}$

Median: $\text{median}\{x\} = \sigma \sqrt{\log(4)}$

Mode: $\text{mode}\{x\} = \sigma$

Variance: $\text{Var}\{x\} = \sigma^2 \frac{4-\pi}{2}$

Second order moment: $E\{x^2\} = 2\sigma^2$

Being $R_i(\sigma^2)$, $i = \{1, \dots, N\}$ a set of random variables with Rayleigh distribution

Maximum Likelihood (ML) estimator

$$\widehat{\sigma^2}_{ML} = \frac{1}{2N} \sum_{i=1}^N R_i^2 = \frac{1}{2} \langle R_i^2 \rangle$$

Unbiased estimator

$$\widehat{\sigma}_c = \sqrt{\frac{2}{\pi}} \frac{1}{N} \sum_{i=1}^N R_i = \sqrt{\frac{2}{\pi}} \langle R_i \rangle$$

ML estimator distribution

- Mean: $E\{\widehat{\sigma}_{ML}^2\} = \alpha\beta = 2\sigma^2$
- Mode: $\text{mode}\{\widehat{\sigma}_{ML}^2\} = (\alpha - 1)\beta = \frac{N-1}{N}2\sigma^2$
- Variance: $\text{Var}\{\widehat{\sigma}_{ML}^2\} = \alpha\beta^2 = \frac{4\sigma^4}{N}$

Unbiased estimator distribution

- Mean: $E\{\widehat{\sigma}_c\} = \sigma\sqrt{\frac{\pi}{2}}$
- Mode: $\text{mode}\{\widehat{\sigma}_c\} \approx \sigma_n\sqrt{\frac{2(2N-1)N}{e}} \approx \sigma_n N\sqrt{\frac{\pi}{2}}$
- Variance: $\text{Var}\{\widehat{\sigma}_c\} = \frac{1}{N}\text{Var}\{R(\sigma)\} = \frac{1}{N}\sigma^2\frac{4-\pi}{2}$

ML estimator distribution

- Mean: $E\{\widehat{\sigma}_{ML}^2\} = \alpha\beta = 2\sigma^2$
- Mode: $\text{mode}\{\widehat{\sigma}_{ML}^2\} = (\alpha - 1)\beta = \frac{N-1}{N}2\sigma^2$
- Variance: $\text{Var}\{\widehat{\sigma}_{ML}^2\} = \alpha\beta^2 = \frac{4\sigma^4}{N}$

Unbiased estimator distribution

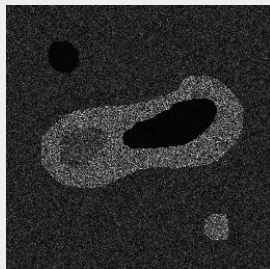
- Mean: $E\{\widehat{\sigma}_c\} = \sigma\sqrt{\frac{\pi}{2}}$
- Mode: $\text{mode}\{\widehat{\sigma}_c\} \approx \sigma_n\sqrt{\frac{2(2N-1)N}{e}} \approx \sigma_n N\sqrt{\frac{\pi}{2}}$
- Variance: $\text{Var}\{\widehat{\sigma}_c\} = \frac{1}{N}\text{Var}\{R(\sigma)\} = \frac{1}{N}\sigma^2\frac{4-\pi}{2}$

If $N \gg$ mean and the mode are approximately equal.

Tissue Identification in Ultrasound Images

- 1 Introduction
 - Speckle
 - Models for Speckle
 - Aim of the work
- 2 Local Statistics of the Rayleigh distribution
 - The Rayleigh distribution
 - Parameter estimation
- 3 Tissue Identification in Ultrasound Images
 - Initial assumptions
 - Algorithm
- 4 Experiments
 - Synthetic Experiments
 - Experiments with Ultrasound Images
- 5 Conclusions

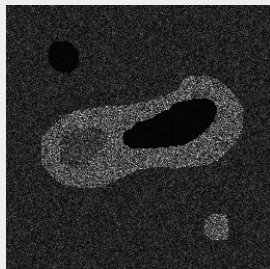
Algorithm: about the image



- Assuming a Rayleigh model for the speckle
- Image model: $\sigma_{ij}^2 = f_{ij}^2 \sigma_n^2$
- Value of σ related to the characteristics of the biological tissue.
- Assumption: each scanned tissue uniform response: similar σ_{ij} for each tissue, and different for different tissues.

Local estimation of sigma allows the identification of different regions belonging to different types of tissues.

Algorithm: about the image



- Assuming a Rayleigh model for the speckle
- Image model: $\sigma_{ij}^2 = f_{ij}^2 \sigma_n^2$
- Value of σ related to the characteristics of the biological tissue.
- Assumption: each scanned tissue uniform response: similar σ_{ij} for each tissue, and different for different tissues.

Local estimation of sigma allows the identification of different regions belonging to different types of tissues.

- 1 Original image estimation using local estimation and assuming Rayleigh distribution.
- 2 Classifying the pixels in tissues
 - 3 Defining the number of classes (tissues).
 - 3 Simple classification algorithm: K-means.

- 1 Original image estimation using local estimation and assuming Rayleigh distribution.
- 2 Classifying the pixels in tissues
 - 3 Defining the number of classes (tissues).
 - 3 Simple classification algorithm: K-means.

- 1 Original image estimation using local estimation and assuming Rayleigh distribution.
- 2 Classifying the pixels in tissues
 - 1 Defining the number of classes (tissues).
 - 2 Simple classification algorithm: K-means.

- 1 Original image estimation using local estimation and assuming Rayleigh distribution.
- 2 Classifying the pixels in tissues
 - 1 Defining the number of classes (tissues).
 - 2 Simple classification algorithm: K-means.

- 1 Original image estimation using local estimation and assuming Rayleigh distribution.
- 2 Classifying the pixels in tissues
 - 1 Defining the number of classes (tissues).
 - 2 Simple classification algorithm: K-means.

Algorithm: image estimators

Mean

$$I_{\hat{\sigma}_{ij}} = \sqrt{\frac{2}{\pi}} \frac{1}{|\eta_{i,j}|} \sum_{p \in \eta_{i,j}} I_p$$

Squared Mean (ML)

$$I_{\hat{\sigma}_{ij}} = \sqrt{\frac{1}{2|\eta_{i,j}|} \sum_{p \in \eta_{i,j}} I_p^2}$$

Median

$$I_{\hat{\sigma}_{ij}} = \sqrt{\frac{1}{\log(4)}} \operatorname{median}_{p \in \eta_{i,j}} \{I_p\}$$

Algorithm: image estimators

Mean

$$I_{\hat{\sigma}_{ij}} = \sqrt{\frac{2}{\pi}} \frac{1}{|\eta_{i,j}|} \sum_{p \in \eta_{i,j}} I_p$$

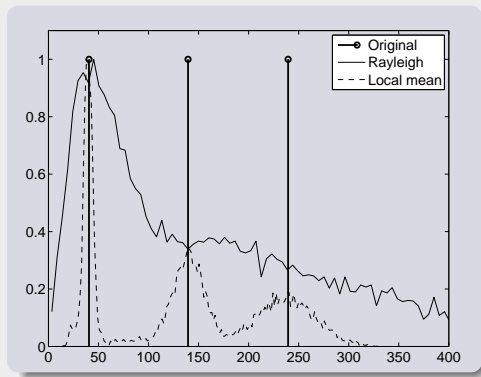
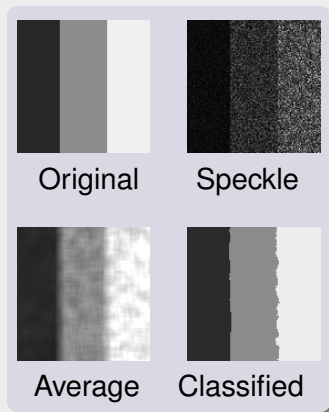
Squared Mean (ML)

$$I_{\hat{\sigma}_{ij}} = \sqrt{\frac{1}{2|\eta_{i,j}|} \sum_{p \in \eta_{i,j}} I_p^2}$$

Median

$$I_{\hat{\sigma}_{ij}} = \sqrt{\frac{1}{\log(4)}} \operatorname{median}_{p \in \eta_{i,j}} \{I_p\}$$

Algorithm: example

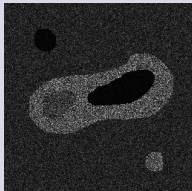


- 1 Introduction
 - Speckle
 - Models for Speckle
 - Aim of the work
- 2 Local Statistics of the Rayleigh distribution
 - The Rayleigh distribution
 - Parameter estimation
- 3 Tissue Identification in Ultrasound Images
 - Initial assumptions
 - Algorithm
- 4 Experiments**
 - **Synthetic Experiments**
 - **Experiments with Ultrasound Images**
- 5 Conclusions

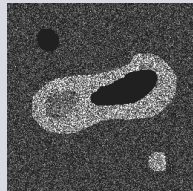
Synthetic Experiments



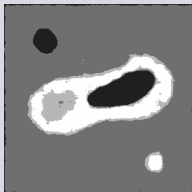
Original Image



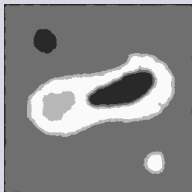
With Speckle (Rayleigh)



Clustering over speckle



Clustering over median

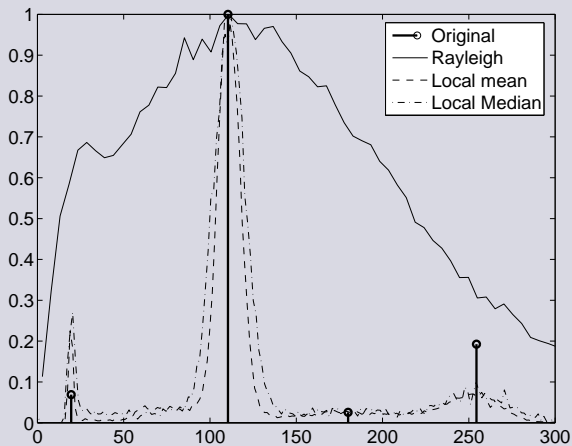


Clustering over mean (9)

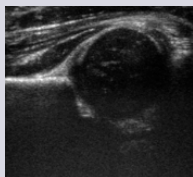


Clustering over mean (5)

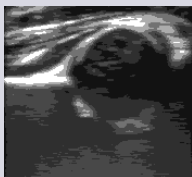
Synthetic Experiments



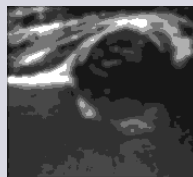
Experiments with Ultrasound Images



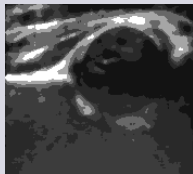
Original



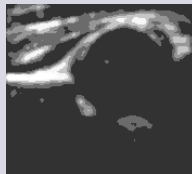
3D mean



2D mean



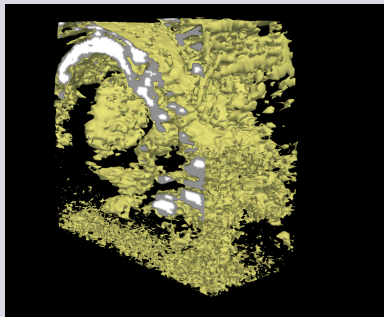
2D median



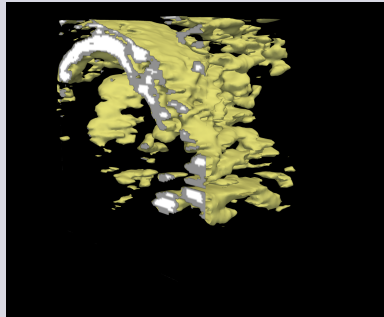
2D squared mean

Experiments with Ultrasound Images

Original



Processed



- 1 Introduction
 - Speckle
 - Models for Speckle
 - Aim of the work
- 2 Local Statistics of the Rayleigh distribution
 - The Rayleigh distribution
 - Parameter estimation
- 3 Tissue Identification in Ultrasound Images
 - Initial assumptions
 - Algorithm
- 4 Experiments
 - Synthetic Experiments
 - Experiments with Ultrasound Images
- 5 Conclusions

Conclusions

- Increase separability of tissues by using local estimators.
- Make any subsequent segmentation easier.
- Clustering done with K-means, (though more complex algorithms may be used).

Future Work

- Adding spatial coherence.
- Using the information for more complex segmentation (Snakes?)
- Other distributions.
- Anisotropic estimation of the parameters.
- Logarithmic compression of the data.

Conclusions

- Increase separability of tissues by using local estimators.
- Make any subsequent segmentation easier.
- Clustering done with K-means, (though more complex algorithms may be used).

Future Work

- Adding spatial coherence.
- Using the information for more complex segmentation (Snakes?)
- Other distributions.
- Anisotropic estimation of the parameters.
- Logarithmic compression of the data.

Thanks for your attention